IN THE SPECIFICATION:

Please amend the specification as follows.

Please amend paragraph [0001] as follows:

RELATED APPLICATIONS

[0001] This application is a continuation of U.S. Patent Application No. 10/020,913, filed on December 19, 2001, which is a continuation in part of U.S. Patent Application No. 09/442,448, filed on January 27, 2000.

Please amend paragraph [0060] as follows:

[0060] The stretching and turning of flexible mesh 37 can be carried out in a convenient manner by using push-pull wires ~~cables~~ 38, shown in Fig. 2. Push-pull wires cables] 38 are sufficiently stiff such that they can carry a tension as well as a compression load, and are attached to tip 40 forming the distal end 4 of catheter 2. Tip 40 can preferably be made of aluminum or plastic. In a preferred example, push-pull wires 38 are made of NITINOL, which is a super-elastic alloy that resists elastic deformation leading to the formation of kinks. For disposable catheters, the wires 38 can alternatively be made of steel, or other materials that tend to regain their original shape after bending. However, NITINOL wires are preferred for applications where catheter 2 is used repeatedly.

Please amend paragraph [0061] as follows:

[0061] Aluminum tip 40, flexible mesh 37, and push-pull wires 38 are all disposed on the circumference of catheter 2, so that working channel 10 is left free for introduction of endoscopy tools. Push-pull wires ~~cables~~ 38 exit the body cavity and exit from catheter 2 at the proximal end 6, and can be either manually controlled or can be controlled by the control unit 34. Control unit 34 controls the steering section 36 in a similar manner as it controls the propulsion section 22.

Please amend paragraph [0063] as follows:

[0063] Devices other than sutures 42 can be used to hold push-pull wires 38 in position around steering section 36. For example, rigid rings can be fixed at axial locations along the steering section 36, and the push-pull wires 38 can be attached to the rings, or may be threaded through holes formed in the ring's outer portion. Alternatively, simple clips or loops can be used to tie push-pull wires 38 to specific points of mesh 37, so the wires can move only in the axial direction. Heat shrink, polyurethane, or other type of low friction flexible cladding can be applied on top of flexible mesh 37 and wires 38 to facilitate insertion and travel of the device within the body cavity. The use of a slippery coating for the catheter makes it easier for the propulsion section 22 to pull the catheter along the body cavity, and also reduces reduce] discomfort to the patient. The low friction coating can also be used on the inside of the cladding, to reduce friction with push-pull wires 38.

Please amend paragraph [0090], on page 18, as follows:

[0090] In certain applications, it may be desirable to apply suction to only a portion of the circumference of suction ring 100. Fig. 11 shows one example of such application, where a perforated sector 106 extends over an arc of approximately 85 degrees [deg.], and the rest of suction ring 100 is not perforated. As described above, the pattern and size of holes 102 can be optimized as desired. In addition, various features also described above can be included in this design, such as axial ridges 122 shown in Fig. 12, and a recessed construction of perforated sector 106, shown in Fig. 13. As before, the purpose of these features is to maximize traction and prevent separation of the entire suction ring 100 from the body cavity tissue.

Please amend paragraph [0105] as follows:

[0105] A drive system is used to cause the flexible tube 304 to translate relative to the body cavity. In one embodiment, a fluid is provided inside of flexible tube 304. The fluid is pressurized so that flexible tube 304 is kept somewhat rigid, and to provide a force that pushes fold 310 away from anchor 312. For example, a pressurization system 314 can provide fluid pressurized by a pump that is conveyed to flexible tube 304 by fluid distribution lines 316. A control unit 320 can be used, for example, to operate the pressurization system 314 via control lines 322. In one exemplary embodiment, a greater fluid pressure can be applied to the portion of the flexible tube 304 between anchor 312 and fold 310, so that the pressure forces fold 310 to translate away from anchor 312. In this exemplary embodiment, one ~~One~~ skilled in the art would appreciate that a seal ~~(not shown)~~ 328 attached to the outer portion 309 and abutting the inner portion 308, such that inner portion 308 can slidably translate adjacent the seal, would permit the pressure force to translate fold 310 away from anchor 312.

Please amend paragraph [0107] as follows:

[0107] In one exemplary embodiment shown in Figure 22, a thrust collar ~~322~~ 327 is attached to catheter 2, and is shaped to receive the fold 310 of flexible tube 304. In this manner, as fold 310 is forced away from anchor 312, a force is applied to thrust collar ~~322~~ 327, and the entire catheter 2 slidably translates in a direction away from anchor 312. In one embodiment, the fluid that pressurizes flexible tube 304 is a lubricant used to facilitate movement of the inner and outer portions 308, 309 relative to each other, and relative to ~~each~~ other~~, and relative to other~~ components of the everting tube.

Please amend paragraph [0110] as follows:

[0110] In one embodiment, the everting tube can be manufactured from a material having azotropic properties, so that it will stretch in one direction, but resist stretching in the perpendicular direction. For example, the everting tube can be made of Silicone, PTFE or PE. The everting tube can be made with or without reinforcing material such as a braid 329.